

1 **Validation of an opto-electronic instrument for the measurement of execution velocity**
2 **in squat**

3

4 **Abstract**

5 The purpose of this study was to analyse the reliability and validity of an opto-electronic
6 sensor system (Velowin) for assessment of the bar-velocity in the deep squat exercise.
7 Mean velocity, mean propulsive velocity and peak velocity generated in the deep squat
8 exercise performed in the Smith machine bar were analysed compared to a linear velocity
9 transducer considered as the gold standard. The study was conducted with a sample of 26
10 men with experience in resistance training. Six measurements were analysed for squat
11 exercise in concentric phase using the a progressive loading increase. Three consecutive
12 repetitions were performed per load with a 3-4 minutes recovery between loads. Analysis of
13 variance confirmed that there were no significant differences ($p >0.05$) for the velocity
14 variables between Velowin and T-Force for each of the loads. The reliability analysis
15 showed high values of the intraclass correlation coefficient (ICC = 0.94-0.99), an "almost
16 perfect" Lin's concordance coefficient (CCC = 0.99) and a low coefficient of variation (CV
17 <3.4%) for each of the loads and velocities. These results confirm the reliability and
18 validity of the Velowin device for measuring the execution velocity in deep squat exercise.

19

20 **Word account:** 190

21 **Key words:** strength; reliability; evaluation; performance; velocity-based training

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23

24 **Introduction**

25 Velocity-based resistance training has implied a paradigm shift in the way programming,
26 control and assessment of resistance training has been conceived lately (González-Badillo
27 et al., 2017b). However, velocity control requires the use of sufficiently reliable measuring
28 instruments.

29

30 Execution velocity monitoring of the most common exercises in strength training
31 has generated scientific interest, showing as its main finding a close relationship between
32 the relative magnitude of the load (%1RM) and the execution velocity with each
33 percentage, being this velocity specific for each exercise (Conceição et al., 2016; González-
34 Badillo & Sánchez-Medina, 2010; González-Badillo et al., 2011; González-Badillo et al.,
35 2014; González-Badillo et al., 2017a). In addition, some researchers maintain that this
36 relationship is very stable regardless of the modifications of the 1RM and the training
37 experience of the subjects (González-Badillo et al., 2017a; González-Badillo et al., 2017b).
38 It is known that the fastest repetition velocity attained during a set in the presence of an
39 absolute load can be used as a good estimator of the relative intensity that this resistance
40 represents at each moment with each exercise (González-Badillo & Sánchez-Medina, 2010;
41 González-Badillo et al., 2011; Sánchez-Medina et al., 2017). More recently, it has been
42 proven that the mean velocity loss during the set is a reliable and quantifiable indicator that
43 reflects the induced neuromuscular fatigue degree (Sánchez-Medina & González-Badillo,
44 2011; Pareja-Blanco et al., 2016), and therefore can be used as a variable to monitor
45 resistance training and adjust the set load (González-Badillo et al., 2017b).

46

47 The importance of accurate velocity measurement lies in the fact that both the
48 neuromuscular requirements and the training effects are largely conditioned by the
49 concentric velocity at which training loads move (González-Badillo et al., 2014).
50 Fortunately, due to growing technological advance, it is now possible to monitor execution
51 velocity and other kinematic parameters through different devices, such as linear velocity
52 or position transducers, video-analysis, accelerometers, and smartphone apps (Sato et al.,
53 2009; Sánchez-Medina & González-Badillo, 2011; Balsalobre-Fernández et al., 2016;
54 Balsalobre-Fernández et al., 2017; Comstock et al., 2011). Among all these instruments, the
55 linear velocity or position transducers are considered by different researchers as reference
56 gold-standard devices for measuring the bar execution velocity in linear movements
57 (González-Badillo & Sánchez-Medina, 2010; Cormie et al., 2007a). Recently, a type of
58 "optical" transducer has been developed (Velowin, Deportec, Murcia, Spain). This novel
59 device can directly measure the position of any body-point at any time frame by means of
60 an infrared camera, which allows to obtain the different velocity variables by derivation for
61 any type of linear trajectory of the load, showing the records of the most determining
62 variables (displacement, phase times, power, etc.) in real time through a graphic and
63 numerical analysis accomplished by its own software. So, this device could overcome some
64 limitations and drawbacks of other type of electronic instruments when measuring
65 execution velocity, such as moderate relative reliability of accelerometer systems (Banyard
66 et al., 2017), low sampling frequency, not discriminating mean propulsive velocity, and not
67 measuring displacement or eccentric action variables (i.e.: smartphone apps and
68 accelerometry-based devices). Specifically, this opto-electronic device has the advantage
69 with respect to the linear velocity or position transducers of not having any extendable

70 cable to fix to the bar or load to move, allowing to assess a wide range of exercises,
71 including the possibility of measuring changes of position (velocity) of any body segment.
72 Despite the possible advantages of this new device, its validation is a prerequisite in order
73 to use this tool with confidence for velocity monitoring.

74

75 Therefore, the objective of this study was to analyse the reliability and validity of an
76 opto-electronic sensor system (Velowin) for assessment of the bar-velocity in the deep
77 squat exercise. For this purpose, execution velocity performed in the Smith machine bar
78 was analysed compared to a linear velocity transducer (T-Force System) considered as the
79 gold standard. In this regard, it was hypothesized that the Velowin opto-electric system is
80 reliable and valid for recording kinematic variables (mean, mean propulsive and peak
81 velocity) compared to the T-Force System linear velocity transducer.

82

83 **Methods**

84 **Experimental design**

85 A unifactorial intra-subject design was used, in which all the participants execute the same
86 deep back-loaded squat exercise (SQ) to obtain mean velocity (MV), mean propulsive
87 velocity (MPV) and maximal or peak velocity (PV) data measured with the Velowin opto-
88 electronic device and the T-Force linear velocity transducer. This was done with the aim of
89 comparing the behavior of both devices for the SQ exercise, taking as independent variable
90 both devices, and as dependent variables the MV (average bar velocity during the entire
91 concentric phase in m/s^2), the MPV (average bar velocity of the propulsive phase, defined
92 as the portion of the concentric action during which acceleration (a) experienced by the

93 moving load is greater than acceleration due to gravity, i.e., $a \geq -9.81 \text{ m}\cdot\text{s}^{-2}$) (Sánchez-
94 Medina et al., 2010) and the PV (maximal instantaneous bar velocity reached at a particular
95 instant during the concentric phase in m/s^2). In this way, the opto-electronic device
96 reliability to measure the exposed kinematic parameters could be tested. The investigation
97 statistical power was evaluated with the statistical program G*Power 3.1.9.2.

98

99 *Participants*

100 The study sample included 26 men (age 29.8 ± 3.5 years, height 178 ± 6.5 cm, body mass
101 75.7 ± 7.6 kg) with experience in resistance training and familiar with the SQ exercise. The
102 established inclusion criteria were: i) to practice intense and/or moderate physical activity
103 at least 2-3 days a week, ii) to have accumulated experience in resistance training with
104 isoinertial equipment ≥ 3 years in order to minimize the bias of variability by differences in
105 technical performance, and iii) not having suffered muscle or bone injury in shoulder,
106 spine, hip, knee, and/or ankle at least six months prior to the study. Likewise, the
107 participants could not have performed any type of intense physical exercise that involved
108 the lower limbs at least 48 hours prior to the measurement day.

109

110 The present study met the ethical standards (Harriss et al., 2017) and was approved
111 by the Research Ethics Commission of the University of Murcia. The study's volunteer
112 participants were informed of risks, purpose and procedures of the research before signing
113 an institutionally approved informed consent document prior to the beginning of the
114 evaluation sessions.

115

116 ***Instruments***

117 The SQ exercise was performed on a Smith machine (Instruments and Sports Technology
118 SL, Murcia, Spain) without any counterweight mechanism, and the reflective marker of the
119 infrared camera of the opto-electronic device (Velowin v.1.7.232, Instruments and Sports
120 Technology; Murcia, Spain) was fixed at the end of the bar along with the extendable cable
121 of the linear velocity transducer (T-Force System, v 2.35; Ergotech Consulting, Murcia,
122 Spain) at the vertical projection of the bar. A complete description of the T-Force System
123 linear velocity transducer is reported elsewhere (Sánchez-Medina & González-Badillo,
124 2011).

125

126 The opto-electronic system and the linear velocity transducer collected the MV,
127 MPV and PV data instantaneously and simultaneously with a frequency of 500 and 1000
128 Hz, respectively, and smoothed the signal using a 4th order lowpass Butterworth filter with
129 no phase shift and 10 Hz cutoff frequency. The opto-electronic instrument calibration was
130 performed according to the manufacturer's instructions. The calculations of the different
131 variables analysed (MV, MPV and PV) are automatically made with the algorithms of each
132 software (Velowin v.1.7.232 and T-Force System v. 2.35, respectively).

133

134 insert here Figure 1

135

136 ***Testing procedures***

137 The participants of the investigation made all the SQ exercise measurements in a force-
138 analysis laboratory (Murcia University, Spain). All tests were performed by the same

139 evaluator, at the same time and under similar environmental conditions (absolute
140 atmospheric pressure 1003 hPa, relative humidity ~60%, height 95 m above sea level and
141 temperature ~24°C).

142

143 The standardized warm-up consisted of 5 minutes jogging, joint mobility exercises
144 and dynamic stretching followed by three sets with a low number of repetitions of the SQ
145 exercise in the Smith machine and a 20, 30 and 40 kg load, respectively. From there, the
146 velocity data record for the SQ exercise was established by a progressive overload with the
147 following dynamics for all participants (Table 1): initial load of the bar (20 kg), with an
148 increase of 10 kg up to 70 kg, for each of the consecutive measurements. Three consecutive
149 repetitions were made for each load. When the execution was considered incorrect (see
150 criteria below), the set was discarded and another one was repeated with the same load after
151 the established recovery interval. The recovery between each set with each load was 3-4
152 minutes.

153

154 An experienced evaluator supervised the subject correct starting position and the
155 technical execution of the exercise. The initial position of the exercise was standing with
156 knees and hips fully extended, feet about shoulder-width apart, and the bar resting on the
157 upper part of the back at acromion level. A line drawn on the ground in the vertical
158 projection of the Smith machine guide rods established the position of the feet metatarsus.
159 Participants were instructed to hold the bar with a grip slightly greater than the width of the
160 shoulders. The displacement of the eccentric phase had to overcome the horizontal plane
161 with the upper part of the thighs, and the knees should be flexed at a tibio-femoral angle of

162 less than 45° in the sagittal plane. The participants were instructed to perform the eccentric
163 phase at a controlled velocity (0.45-0.75 m/s²) with the real-time visual and acoustic
164 feedback help provided by the linear velocity transducer software and, from that point,
165 execute the concentric phase at the maximal possible velocity up to the initial position.
166 Strong verbal encouragement was provided to perform the maximum effort (the instruction
167 provided to the participants was "push as fast as you can"). It was required that the feet
168 were in constant contact with the ground throughout the execution, although the heels were
169 allowed to rise at the end of the concentric phase with lighter loads. It was not allowed to
170 take off the bar resting on the shoulders during the braking phase of the concentric
171 movement.

172

173 insert here Table 1

174

175 **Statistical analyses**

176 For analysis of the data, only the fastest repetition of each load of the evaluated velocity
177 variables was selected. The data analysis was performed using the statistical program SPSS
178 (IBM SPSS version 21.0, Chicago, IL, USA). All variables met the assumption of
179 normality (Shapiro-Wilk test). Data are presented as means ± standard deviation. In
180 addition, the confidence intervals (CI) were further calculated for all bar-velocity outcomes
181 in each load. Analysis of variance (ANOVA) was performed to verify the existence of
182 significant differences between both devices in the means of each variable analysed. The
183 calculation of the reliability was obtained through the Intraclass Correlation Coefficient
184 (ICC), the Coefficient of Variation (CV) and the Lin's Concordance Correlation Coefficient

185 (CCC). Acceptable reliability was determined as an ICC > 0.75 and a CV < 10%. However,
186 the Standard Error of the Measurement (SEM), the CV and the ICC have some limitations
187 in that very high values can be obtained (close to 1) even though there are important
188 differences between the measurements (if observed in a scatter plot), these being non-
189 concordant. For this reason, Lin (Lin, 1989) developed a proposal to evaluate the strength
190 of concordance or agreement between continuous variables in a more demanding way
191 through the concordance-correlation coefficient. This coefficient is defined as the product
192 of precision -represented by the correlation coefficient- and accuracy -represented by the
193 bias correction coefficient. Lin revealed that this method used to evaluate the
194 reproducibility of measurements is superior to others (mentioned above) which are used for
195 similar purposes. Values for CCC are classified as: "almost perfect" >0.99, "substantial"
196 between 0.95 and 0.99, "moderate" between 0.90 and .95, and "poor" <0.90 (Cortés-Reyes
197 et al., 2010). A significance level of $p < 0.05$ was accepted for all the analysis.

198

199 **Results**

200 *Preliminary test of normality*

201 *Shapiro Wilk test* was used to verify the normality of the MV, MPV and PV variables with
202 each of the loads evaluated in both devices (Velowin and T-Force). The test confirmed that
203 all the variables have a normal distribution of $p > 0.05$, except the mean velocity ($p = 0.17$
204 for velowin and $p = 0.02$ for T-Force) and the mean propulsive velocity ($p = 0.03$ for
205 velowin and $p = 0.03$ for T-Force) in the first repetition (ST1) with the 20 kg load.
206 Skewness and kurtosis values were between 0 and 2.

207

208 ***Reliability***

209 ICC shows a mean value of 0.98 and values from 0.94 to 0.99 (95% CI) based on the MV,
210 MPV or PV variable for Velowin and T-Force. The Pearson correlation coefficient showed
211 values from $r \geq 0.70$ to $r = 0.96$. CV values for the analysed variables with each one of the
212 loads were less than 3.4% (Table 2).

213 CCC values show an "almost perfect" agreement or concordance with all analysed
214 loads and velocity variables (CCC = 0.99; CCC = 0.98 for MV with 20 kg). This
215 corroborates the concordance (precision and accuracy) of the measurement in the Velowin
216 device for MV, MPV and PV kinematic variables in SQ exercise.

217

218 insert here Table 2

219

220 ***Validity***

221 **Standard statistical mean and standard deviation for Velowin and T-Force in Squat**
222 **exercise.**

223 Mean values \pm SD of the velocities for Velowin and T-Force devices are summarized
224 (Table 3). Mean values are similar in both devices for each of the velocities analysed with
225 the different loads.

226

227 insert here Table 3

228

229 **Analysis of variance (ANOVA) for mean velocity, mean propulsive velocity and peak**
230 **velocity variables for Velowin and T-Force in Squat exercise.**

231 To analyse the existence of significant differences in the total scores of MV, MPV and PV
232 an ANOVA was performed considering velocity outcomes as dependent variables and the
233 "Test" variable as an independent variable with two levels (Test 1 = Velowin, Test 2 = T-
234 Force). The variances are homogeneous (*Levene test*) $p > 0.05$ and no significant
235 differences were found between the variances of the two devices.

236

237 **Discussion and implications**

238 According to the obtained results, the hypothesis of reliability and validity of the opto-
239 electric device to measure execution velocity in squat exercise was confirmed. To the best
240 of our knowledge, this is the first scientific study that aimed to validate the Velowin
241 camera-based opto-electronic device by comparing it with a linear velocity transducer as a
242 reference instrument for the variables of MV, MPV and PV in deep squat exercise
243 conducted in a Smith machine.

244

245 Research has shown that monitoring repetition velocity is an objective, real time,
246 and noninvasive indicator of relative intensity (from fastest repetition velocity attained
247 during a set), the number or percentage of repetitions performed (using the magnitude of
248 velocity loss attained in the set) and the muscle fatigue during resistance training
249 (González-Badillo & Sánchez-Medina, 2010; González-Badillo et al., 2011, González-
250 Badillo et al., 2017a). Accordingly, the importance of accurately assessing bar-velocity for
251 strength training prescription and load control purposes is essential. In this sense, some data
252 sustain that differences of mean propulsive velocity as small as 0.07-0.09 m/s² against the
253 same absolute load can represent variations of approximately 5% of the relative training

254 intensity (González-Badillo & Sánchez-Medina, 2010; González-Badillo et al., 2017b). For
255 this reason, the validation of this novel device is important as it presents some advantages
256 and could overcome some limitations of other type of electronic instruments for measuring
257 execution velocity.

258

259 Criterion-related validation requires to know the correlation between a criterion and
260 an instrument working simultaneously, and which allows the replacement of the more
261 complex criterion for another (instrument) that is simpler or more accessible. For this
262 purpose, the choice of criterion is critical (Sato et al., 2009). When the degree of measure
263 agreement between two instruments is known, it can be established whether or not they can
264 be validated, and therefore if they can be interchanged for the measurement of certain
265 variables. In this line, the analysis of relative reliability measures shows very high values in
266 the Intraclass Correlation Coefficient (ICC = 0.94-0.99) for both devices with different
267 loads for velocity variables. Although there are no pre-established standards for reliability
268 measures of concurrent validation studies, it has been suggested that ICC values above 0.75
269 can be considered reliable, and that this index should be at least 0.90 for most clinical
270 applications (Thomas, 2005). Likewise, the values of the Coefficient of Variation for the
271 same variables demonstrate a good absolute reliability (CV <3.4%) with different loads.
272 Scientific literature suggests that the coefficient of variation should be lower than 10%,
273 although these estimates have been a source of discrepancy (Atkinson & Nevill, 1998;
274 Cronin et al., 2004). In the same way, the Lin's concordance correlation coefficient shows
275 an "almost perfect" agreement or concordance in all analysed loads and velocity variables
276 (CCC = 0.99). According to Lin et al. (Lin, 1989) CCC is the most relevant and adequate

277 statistical correlation test used in validation studies to confirm the accuracy and precision of
278 an instrument for continuous numerical variables (in this case MV, MPV and PV). All
279 these data together corroborate the measurement accuracy of the Velowin device for the
280 kinematic variables of mean velocity, mean propulsive velocity and peak velocity in the SQ
281 exercise. In addition, having used a Smith machine for velocity measurement could help
282 reduce the measurement error both random and systematic. Since the free weight squat
283 exercise does not follow a strictly linear trajectory (Rudner et al., 2003), the use of a Smith
284 machine is recommended to restrict the displacement of the bar to the vertical direction in
285 this validation study. In fact, data derived from horizontal oscillations of the bar outside the
286 vertical vector can modify the data and can alter the accuracy of the vertical velocity
287 evaluation (Cormie et al., 2007a).

288

289 Validity is generally referred to as the ability of a measurement tool to reflect what
290 it is designed to measure (Atkinson & Nevill, 1998). In the presence of a standard measure
291 it is particularly useful to establish criterion validity, which evaluates the degree to which
292 the scores of a test are in relation to some recognized standards (Sato et al., 2009). In this
293 sense, an adequate criterion validity of the Velowin device is confirmed with respect to the
294 "gold standard" (linear velocity transducer). The analysis of variance (one-way ANOVA)
295 showed that there were no significant differences ($p > 0.05$) in MV, MPV and PV
296 measurements for each of the recorded loads with the Velowin and the T-Force device in
297 deep squat exercise, indicating that they measure in a similar way.

298

299 The linear velocity or position transducers are considered by different researchers to
300 be the reference instruments for measuring the bar execution velocity in linear movements
301 (González-Badillo & Sánchez-Medina, 2010; Cormie et al., 2007a). These devices are
302 electromechanical measuring instruments, since the transducer output is usually an electric
303 signal such as voltage or electric current intensity (González-Badillo et al., 2017b; Harris et
304 al., 2010). All of them have an extendable cable that is attached to the moving external
305 resistance. Depending on the linear velocity changes of cable displacement or the changes
306 in position, as a function of time, the rest of the kinematic (acceleration) and dynamic
307 variables (force, power) are derived (González-Badillo et al., 2017b). These devices require
308 the trajectory of the bar movement to be linear so that the recording is as reliable and
309 accurate as possible (Sánchez-Medina & González-Badillo, 2011; Harris et al., 2010).
310 Specifically, the linear velocity transducer used for this study as a "gold-standard" (T-Force
311 System) has been widely used to evaluate kinetic and kinematic variables in resistance
312 exercises (González-Badillo & Sánchez-Medina, 2010; González-Badillo et al., 2011;
313 González-Badillo et al., 2014; González-Badillo et al., 2017; Sánchez-Medina and
314 González-Badillo, 2011; Pareja-Blanco et al., 2016; Sánchez-Medina et al., 2017). The high
315 reliability (ICC = 1.00, CV = 0.57%) and validity of this instrument have been previously
316 described (Sánchez-Medina & González-Badillo, 2011). In addition, having used a linear
317 transducer for direct measurement of velocity as a criterion for this study reduces the
318 possible error generated by the mathematical derivation made by linear position transducers
319 in the estimation of velocity according to time (Harris et al., 2010). Likewise, the T-Force
320 transducer has a high sampling frequency (1000 Hz), which is essential to correctly detect

321 the starting and ending moment of each repetition performed, as well as to accurately
322 obtain the peak values and derived variables (González-Badillo et al., 2017b).

323

324 We are not aware of any validation study that has used a position opto-electronic
325 device to measure execution velocity in exercises with linear trajectories such as the squat
326 conducted in a Smith machine. A validation study of a linear position transducer, which
327 used the bench press and squat exercises, was able to verify the high reliability (ICC = .85-
328 .98) and the low to moderate systematic and random error of peak velocity, mean velocity,
329 and mean power variables with respect to the same linear velocity transducer used in our
330 study as reference (Garnacho-Castaño et al., 2015), but could not compare mean propulsive
331 velocity data since the linear position transducer analysed does not have this data. Other
332 validation studies of linear position transducers have used force platforms (Cormie et al.,
333 2007b; Crewther et al., 2011) or video-analysis (Drinkwater et al. 2007) as a criterion to
334 study force and power values in different jumps and other resistance exercises, but none of
335 them analysed velocity variables with which to compare the results of our study.

336

337 On the other hand, in recent years different studies have been published on the
338 reliability and concurrent validity of accelerometry-based devices and smartphone apps
339 (Sato et al., 2009; Balsalobre-Fernández et al., 2016; Balsalobre-Fernández et al., 2017;
340 Comstock et al., 2011) for measuring execution velocity. Although these studies generally
341 show a high correlation of mean and peak velocity with those recorded by the linear
342 position transducer used as a reference ($r = 0.86$; $r = 0.98$, respectively) (Balsalobre-
343 Fernández et al., 2016), the peak and mean velocity values are slightly lower (-0.07 ± 0.1

344 m/s²) and higher (0.11 ± 0.1 m/s²), respectively, than the transducer used for each study in
345 the analysed exercises, both for accelerometers (Balsalobre-Fernández et al., 2016) as for
346 the video-analysis through app (Balsalobre-Fernández et al., 2017). A recent validation
347 study that compared an accelerometer system and a linear position transducer with a force
348 platform and other linear transducers during the free weight squat exercise concluded that
349 only the linear position transducer was reliable enough for velocity measurements (Banyard
350 et al, 2017). It has been described that accelerometry-based devices provide velocity values
351 with great error, especially when working with low or very high loads (González-Badillo et
352 al., 2017b), which discourages their use when it is intended to collect data accurately and
353 correctly interpret the effects of training. Therefore, since velocity outcomes recorded by
354 the accelerometry-based devices are not "real" in absolute terms, compared to those
355 recorded by linear position transducers, they are not interchangeable instruments
356 (Balsalobre-Fernández et al., 2016; Balsalobre-Fernández et al., 2017). It is also important
357 to note that none of the validation studies of the aforementioned devices has been based on
358 Lin's correlation-concordance coefficient as a statistical indicator to analyse reliability.

359

360 Another remarkable issue is the fact that the Velowin opto-electronic device used
361 for this study is capable of measuring MPV, that is, the portion of the movement during
362 which the applied force is positive (>0) (González-Badillo et al., 2017b). By contrast, no
363 current wearable device (accelerometers and apps) allows discriminating mean velocity of
364 the *propulsive* phase, that is, mean values of the "propulsive" phase of the concentric
365 action. According to some authors, this velocity variable is probably the most relevant in
366 the analysis of load programming and assessment of the training effect on performance,

367 since it better discriminates the potential or neuromuscular ability of subjects at low and
368 medium loads (González-Badillo et al., 2017b; Sánchez-Medina et al., 2010). Furthermore,
369 for the precise calculation of the propulsive phase duration of each repetition - and,
370 therefore, of the mean propulsive velocity - it is necessary to have devices with a sampling
371 frequency of at least 500 Hz, since, without a high sampling frequency and a very accurate
372 acceleration value, the propulsive phase cannot be adequately determined (González-
373 Badillo et al., 2017b). Lastly, this opto-electronic device has the advantage with respect to
374 the gold standard of not having any extendable cable to fix to the load to move, allowing to
375 assess a wide range of exercises (i.e. vertical jumps, machine exercises), including the
376 possibility of measuring changes of velocity (position) of any body segment. Nevertheless,
377 we consider that this novel device should improve other aspects to facilitate its usability: a
378 simpler calibration procedure and an electric self-feeding system.

379

380 **Conclusions**

381 The main finding of this study was the high reliability and concurrent validation of the
382 Velowin opto-electronic system for measuring the execution velocity. In this regard, this
383 tool could be useful for training, monitoring and assessing the performance of resistance
384 exercises with linear trajectories such as squat. This study shows that it is possible to
385 control and assess neuromuscular performance, using execution velocity in linear resistance
386 training exercises such as squat, in an accessible and effective way by using this
387 measurement system instead of a linear transducer. Opto-electronic technology could
388 become an accessible resource for exercise science professionals working in different

389 contexts who need to accurately assess performance changes in resistance training exercises
390 through execution velocity.

391

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