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**Viscoelastic properties of the central region of porcine temporomandibular joint disc in shear stress-relaxation.**

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1 **Abstract**

2 In this study, the shear relaxation properties of the porcine temporomandibular joint  
3 (TMJ) disc are investigated. Previous studies have shown that, in fatigue failure and  
4 damage of cartilage and fibrocartilage, shear loads could be one of the biggest  
5 contributors to the failure. The aim of the present study is to develop an evaluation  
6 method to study shear properties of the disc and to do a mathematical characterization  
7 of it. For the experiments, twelve porcine discs were used. Each disc was dissected  
8 from the TMJ and, then, static strain control tests were carried out to obtain the shear  
9 relaxation modulus for the central region of the discs. From the results, it was found  
10 that the disc presents a viscoelastic behavior under shear loads. Relaxation modulus  
11 decreased with time. Shear relaxation was 10% of the instantaneous stress, which  
12 implies that the viscous properties of the disc cannot be neglected. The present results  
13 lead to a better understanding of the discs mechanical behavior under realistic TMJ  
14 working conditions.

15

16 **Keywords:** Temporomandibular Joint; Soft Tissues; Viscoelasticity; Biomechanical  
17 Characterization; Experimental Techniques; Shear.

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## 1        **1. Introduction**

2        Synovial joints allow various degrees of relative motion among the bones to be  
3        regulated by muscles attached to the latter (Widegren et al., 2000). Daily activity  
4        accompanies joint motion resulting in joint loads. The temporomandibular joint (TMJ),  
5        a diarthrodial synovial joint, enables large relative movements between the temporal  
6        bone and the mandibular condyle (Rees, 1954; Scapino et al., 2006). Within the joint,  
7        both the articular surfaces of the condyle and temporal bone are covered by a thin  
8        fibro-cartilaginous layer showing a very low coefficient of friction (Tanaka et al., 2004b).  
9        A dense fibrocartilaginous articular disc is located between the bones in each TMJ.  
10       The disc provides a largely passive movable articular surface accommodating the  
11       traslatory movement made by the condyle (Koolstra and Tanaka, 2009).

12       The TMJ disc has an important load-bearing, stress absorbing and joint stabilizing  
13       function (Barrientos et al., 2016; Fernández et al., 2013; Tanaka et al., 2008; Tanaka  
14       and Eijden, 2003). The disc is subject to various types of loading, such as sustained  
15       loading during clenching and intermittent loading during mastication (Hattori-Hara et  
16       al., 2014; Hirose et al., 2006; Tanaka et al., 2007). Stresses are divided into  
17       compression, tension and shear components. During every type of loading the disc  
18       undergoes a deformation while internal forces arise within the tissue. The  
19       viscoelasticity of such a material, as that of the disc, is the principal factor of energy  
20       dissipation (Fung, 1969). These types of tissues show different mechanism of energy  
21       dissipation that are result of the different phases in their structure: interstitial fluid flow  
22       within and through the matrix and relaxation of the solid matrix (collagen fibers and  
23       proteoglycans). Without strain energy dissipation, storage of the exceeding strain  
24       energy can lead to breakage of the articular disc and other components of the TMJ  
25       (Tanaka et al., 1999).

1 Since shear stress can result in fatigue, damage and deformation of cartilage,  
2 investigation of shear properties in synovial joints is of particular interest (Spirt et al.,  
3 2005; Zhu et al., 1993, 1994). Gallo et al. (2000) suggest that, during mastication,  
4 fatigue failure of the TMJ disc could result from shear stresses caused by medio-lateral  
5 translation of stress location. Therefore, data on the shear modulus might contribute  
6 to a better understanding of secondary tissue damage. It has been reported that the  
7 shear stress in cartilage is very sensitive to the frequency and direction of the loading  
8 and to the amount of compressive strain (Mow et al., 1992). However, in the literature  
9 few studies are available in which the viscoelastic properties of the TMJ disc are  
10 measured in shear stress-relaxation.

11 This paper may provide better insight about the possible mechanism leading to tissue  
12 fatigue and failure due to shear. Therefore, in this study the viscoelastic properties of  
13 porcine TMJ disc are investigated under shear stress relaxation, aiming at advancing  
14 in the design of biomimetic disc substitutes and in the understanding of the pathological  
15 conditions of the TMJ disc.

16

## 17 **2. Materials and Methods**

18 Previous studies have shown that due to morphology, function and diet, pig discs are  
19 the closest to human discs making them an appropriate model for TMJ studies  
20 (Bermejo et al., 1993; Kalpakci et al., 2011). In this study, twelve healthy-looking TMJ  
21 discs from 6 pigs (age: approx. 6–7 months, gender not specified) were obtained at a  
22 local slaughterhouse (Noreña, Asturias, Spain). The protocol of the experiment was  
23 approved by the Animal Care and Use Committee at the University of Oviedo, Spain.  
24 The discs were carefully dissected immediately after the sacrifice, introduced in  
25 hermetic containers immersed in a physiologic saline solution (NaCl 0.09 g/100 ml),

1 and frozen at  $-25\text{ }^{\circ}\text{C}$  for 3 days until the experiment was initiated for testing (Allen and  
2 Athanasiou, 2005; Calvo-Gallego et al., 2017). The discs were completely unfrozen in  
3 a refrigerator at  $3\text{-}4\text{ }^{\circ}\text{C}$  and, then, allow to reach room temperature ( $20\text{ }^{\circ}\text{C}$ ) before  
4 testing. Using a cylindrical  $4.0\text{ mm}$  diameter tissue punch, two experimental specimens  
5 were dissected from the central region of each disc (see Figure 1).

6 Although previous studies have shown region-dependent mechanical properties  
7 (Fernández et al., 2013), this study is only focused on the central region, mainly due  
8 to the complexity of extracting two specimens with the necessary dimensions of the  
9 rest of regions.

10 All the specimens were tested in a DMA Instrument (RSA3, T.A. Instruments, USA) in  
11 unconfined shear using a shear tool (see Figure 2) at room temperature ( $20\text{ }^{\circ}\text{C}$ ). The  
12 loading was applied in the antero-posterior direction, since mechanical properties of  
13 the disc, due to fiber distribution, will also be direction-dependent.

14 As mentioned before, two specimens of each disc were cut. In Figure 2, it can be seen  
15 that the shear-tool has a sandwich configuration and samples need to be place at both  
16 sides of the tool. In order to test shear in antero-posterior direction, the fibers of the  
17 specimens need to be aligned with the movement of the tool (vertical direction),  
18 according to Figure 3.

19 To avoid the specimens to slippage during shear loading, 600 grit sandpaper was glued  
20 to the surfaces of the shear tool. Additionally, the selected inner part of the shear tool  
21 would allow testing  $2\text{ mm}$  thick specimens. Taking into account the average thickness  
22 value for the discs,  $1.84\pm 0.11\text{ mm}$ , and the real gap for testing,  $1.750\text{ mm}$  (subtracting  
23 the sandpaper sheet thickness), an average initial value of 5% pre-strain in the  
24 compression direction was applied before testing. After previous step, a 3-min  
25 preconditioning test was performed with 1% sinusoidal strain before the subsequent

1 shear stress relaxation test. The shear strain was applied to the specimens moving the  
2 lower part of the tool in the axial direction of the machine (vertical direction in Figure 2  
3 and 3). The shear relaxation tests were carried out at strain levels of 5% and 8% to  
4 obtain the corresponding relaxation modulus. The specific level of shear strain was  
5 produced under an instantaneous strain step and kept constant during 120 seconds  
6 for each stress relaxation test keeping the same test procedure used in previous  
7 studies (Barrientos et al., 2016).

8 To apply and maintain the initial value of strain during the relaxation test, the DMTA  
9 machine is equipped with a motor driven by an air bearing system, which applies the  
10 corresponding displacement at a very high rate once the strain is commanded before  
11 testing (T.A.Instruments, 2001). Loads were measured simultaneously under the  
12 specified constant strain.

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### 14 **3. Results**

#### 15 **3.1 Viscoelastic properties of porcine TMJ disc in shear stress relaxation**

16 From the experimental tests, the mean and standard deviation of the shear modulus  
17 of the TMJ disc at convenient times were calculated. The resulting curves for the 5 and  
18 8 % strain levels are presented in Figure 4 (left and right plots, respectively).

19 For comparison proposals both averaged curves are plotted in Figure 5. From Figure  
20 5, a higher shear modulus is observed for the 8 % strain level. From the results (Figure  
21 5), a dependence of the relaxation modulus,  $G(t)$  with applied strain can be observed,  
22 which is in agreement with the TMJ disc behaviour previously observed (Lamela et al.,  
23 2011).

24 The shear modulus obtained for both strain levels (see Figure 5) presents a large  
25 relaxation ratio. For 1 s, the shear modulus decreases about 70% while a 90 %

1 reduction is observed for 100 s.

2

### 3 **3.2 TMJ shear relaxation model**

4 Due to its simplicity, even though other models could be used, generalized Maxwell  
5 model was used to fit the experimental data to the viscoelastic model represented in  
6 Figure 6, as a combination of spring and dashpot elements (Tschoegl, 2012), which  
7 can be modelled using the Prony's series model given by the equation:

$$G(t) = G_0 \left[ 1 - \sum_{i=1}^{n_t} g_i \left( 1 - \exp\left(-\frac{t}{\tau_i}\right) \right) \right] \quad (1)$$

8 where  $g_i$  and  $\tau_i$  are the Prony parameters and  $G_0$  is the instantaneous shear  
9 modulus.

10 To simplify the material model, as well as to take into account the dependence of the  
11  $G(t)$  with the applied strain, a unique set of Prony parameters was used to fit both  
12 shear modulus curves. This procedure profits from the fact that a simple vertical shift  
13 is observed between both material curves (see Figure 5) which could be interpreted as  
14 a proportional shift of  $G(t)$  with the strain.

15 Two steps were used for fitting the material model. Firstly, the shear curves for the  
16 TMJ are averaged and, next, the generalized Maxwell model was applied to fit the  
17 averaged curve by means of the Prony series equation (1).

18 To fit adequately the experimental data, 8 Prony terms were necessary being the R-  
19 square 0.994. The parameters of the Prony series presented in Table 1 define the  
20 normalized viscoelastic curve for the material, as a function of the instantaneous  
21 modulus of the material,  $G_0$ . In this way, the curves for the 5% and the 8% strains are  
22 gained from the fitted model, simply, by multiplying in each case equation (1), by the  
23 corresponding instantaneous modulus. Accordingly,  $G_0^{5\%} = 1.6205e + 04$  kPa and

- 1  $G_0^{8\%} = 1.8883e + 04$  kPa, for the 5 % and the 8 % shear modulus curves, respectively.
- 2 The Prony series parameters with higher precision are included in the appendix.
- 3 Table 1. Prony series parameters ( $R^2=0.994$ ) for the normalized TMJ shear modulus
- 4 curve.

$\tau_i$	$G_i$
3.17e-02	4.14e-01
1.00e-01	7.90e-02
3.19e-01	6.26e-02
1.01e+00	6.36e-02
3.21e+00	5.68e-02
1.01e+01	7.36e-02
3.22e+01	6.65e-02
1.02e+02	1.44e-01

- 5 The experimental and the analytical curves (using equation (1)) are presented in Figure
- 6 7. The maximum error between the experimental results and the proposed model are
- 7 less than a 2% for both curves.

8

#### 9 **4. Discussion**

- 10 Fatigue failure and damage of joint tissues, including both disc and cartilage, may be
- 11 more linked to repeated and prolonged extension and shear motions than to the joint
- 12 compression applied (Iatridis and ap Gwynn, 2004; Tanaka et al., 2003). Even when
- 13 the disc slides along smooth temporal cartilage during jaw movements, shear loading
- 14 of the disc and cartilage has been considered to be negligible due to almost zero
- 15 friction. However, several authors support the evidence that the disc and cartilage are
- 16 subjected to shear stress. For example, after prolonged clenching and grinding, only



1 solid contact may exist between the disc and cartilages, without boundary lubrication  
2 between them, resulting in considerable shear stress (Forster and Fisher, 1999, 1996;  
3 Tanaka et al., 2001). Few studies of the behaviour of the TMJ disc under dynamic  
4 shear loads were performed in the past (Juran et al., 2013; Koolstra et al., 2007;  
5 Tanaka et al., 2004a, 2003) to evaluate the mechanical properties of the disc at  
6 different strain rates and frequencies. The present study is, as far as we know, the first,  
7 in which the shear relaxation properties of the TMJ disc in shear stress relaxation were  
8 examined. Wu et al. (2015) investigated the intrinsic viscoelastic shear properties in  
9 porcine TMJ disc, but in contrast to the present study, they applied a rotational shear  
10 loading. The present design might reproduce the actual environment in the TMJ disc.  
11 In this study, relaxation viscoelastic behaviour of cut specimens is evaluated in antero-  
12 posterior direction at 5 and 8% shear strain levels. As a result, the instantaneous shear  
13 moduli were increased with increasing applied strain. This evidences a dependence  
14 with strain of the behaviour of the disc which is in good agreement with the general  
15 mechanical behaviour observed previously in the TMJ disc (Lamela et al., 2011;  
16 Tanaka and Eijden, 2003). The possible explanation for this increment is the stretching  
17 of collagen fibers in antero-posterior direction (Barrientos et al., 2016; Lamela et al.,  
18 2011; Tanaka et al., 2003). Furthermore, present results show that the relaxed stress  
19 of the porcine TMJ disc was approximately 10% of the instantaneous stress  
20 irrespective of shear strain amplitude. This indicates that energy-dissipation function  
21 takes place in the TMJ disc. Without the energy dissipation capacity of the disc, TMJ  
22 components including bony components and soft tissue probably fail resulting in the  
23 tissue rupture. Thus far, it is concluded that the TMJ disc plays an important role as a  
24 stress bumper during complex mandibular movements.  
25 When comparing the compression relaxation tests (Barrientos et al., 2016; Lamela et

1 al., 2011) with the shear relaxation tests, the present results clearly show that  
2 compression relaxation modulus is 10 times higher than shear relaxation modulus.  
3 Adam et al. (2015) investigated an image-based modelling study on the bovine caudal  
4 disc, and concluded that shear resistance between lamellae confers disc mechanical  
5 resistance to compression. This points out the relationship between shear and  
6 compressive properties of the TMJ disc. Moreover, the present results reveal that the  
7 porcine TMJ discs exhibited shorter relaxation times under shear stress relaxation than  
8 under compressive stress relaxation. This may be due to the difference of an outflow  
9 of interstitial fluid caused by pressurization of the compressed area. During shear  
10 stress relaxation, the fluid within the disc is likely to move along the stretching collagen  
11 fibers; however, during compressive stress relaxation, the disc maintains a fluid  
12 pressure because of sustained interstitial fluids within the disc. Since the load bearing  
13 functions of cartilaginous tissues are mainly provided by the viscoelastic property of  
14 collagen fiber network and the osmotic pressure due to the presence of proteoglycans  
15 (Hardingham and Fosang, 1992), the large proteoglycans and the related chondroitin  
16 sulfate might be more important to counteract compression and shear, while the  
17 collagen fibers are more important to counteract tension (Tanaka and Eijden, 2003).  
18 In literature, authors have used different models to characterize the viscoelastic  
19 properties of the TMJ disc (Allen and Athanasiou, 2006; Tanaka and Eijden, 2003). For  
20 large displacements, other models could be more appropriate (Fung, 1969). In this  
21 study, a generalized Maxwell model, based on Prony's series, was applied to  
22 characterize the shear relaxation modulus of the material. Although the TMJ disc  
23 presents a strain-dependence behavior, almost the same relaxation rate is observed  
24 for the strain levels applied in the experiments (see Figure 5). This fact allows a unique  
25 viscoelastic model to be fitted where the instantaneous modulus  $G_0$  at the

1 corresponding strain level must be used. The results obtained with the proposed Prony  
2 series model can be considered adequate for the shear relaxation modulus of the TMJ  
3 disc showing errors under 2%.

4 To be consistent with previous studies and allowed comparison (Barrientos et al., 2016;  
5 Fernández et al., 2013), some testing conditions, such relaxation time and temperature,  
6 and model parameters were chosen. Temperature affects mechanical results as higher  
7 temperatures reduce stiffness and strength of the discs (Detamore and Athanasiou,  
8 2003).

9 In conclusion, the relaxation properties of the porcine disc were determined under  
10 shear in this study. A method to test the disc under relaxation shear conditions was  
11 proposed. The study shows that the viscoelastic properties of the disc under shear  
12 loads cannot be neglected. Shear properties of the disc in antero-posterior direction  
13 were characterized using a unique Maxwell model. Nevertheless, this study is a first  
14 step in the shear characterization of the TMJ discs and further studies are needed to  
15 conclude on the shear behavior of the disc in medio-lateral direction, cyclic loads, pre-  
16 compression and region dependencies.

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1      **7. Appendix A**

2      Table 1. Prony Series coefficients for the TMJ Shear modulus with higher precision

$\tau_i$	$G_i$
3.171801782714793e-02	4.146791885739055e-01
1.006032675003927e-01	7.901525169602446e-02
3.190936295865514e-01	6.262266247153189e-02
1.012101763417593e+00	6.369962544203969e-02
3.210186241700431e+00	5.687840666168365e-02
1.018207464791342e+01	7.366328040806444e-02
3.229552316589736e+01	6.652140489569733e-02
1.024350000000000e+02	1.443664636944322e-01

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